

### Introduction

EEG alpha rhythm has been used as a neurophysiological measure of activation, ranging from relaxation at rest to task-related local cortical synchronization or desynchronization. Although the topographic capacity of high density EEG is limited by volume conduction, it is enhanced by CSD transformation, which provides reference-free measures that represent the neuronal generator pattern underlying alpha. CSD-based frequency principal components analysis (CSD-tPCA) of resting EEG has identified posterior, condition-dependent (eyes closed-minus-open) alpha as a predictor of treatment response to serotonergic antidepressants.<sup>[9]</sup> Serotonergic and dual treatments (serotonergic plus bupropion, an NDRI) did not differ as both responder groups showed greater posterior alpha. However, this study tested only a limited number of patients treated with bupropion alone. Moreover, task-related alpha also varies during the performance of behavioral tasks, and these changes may be quantified as event-related spectral perturbations (ERSP). The present 67-channel EEG study combined task-related (novelty oddball) and resting CSD alpha measures obtained from depressed patients prior to treatment with a serotonergic antidepressant ( $n = 77$ ) or bupropion alone ( $n = 23$ ).

### Methods

**Participants.** Depressed patients ( $n = 127$ ; 60 male; age  $38.3 \pm 11.8$  yrs) and healthy adults ( $n = 114$ ; 54 male;  $31.2 \pm 10.0$  yrs) with no history of any psychopathology or neurological disorder.

**Novelty Oddball Task.** An auditory novelty oddball task<sup>[6]</sup> consisted of eight 50-trial blocks of 300-ms tones (10 ms rise and fall time) and novel sounds (100-400 ms duration) presented in pseudorandom order (1000 ms SOA). Unique novel sounds (e.g., animals, instruments;  $p = .12$ ) were intermixed with frequent nontargets (350 Hz;  $p = .76$ ) and infrequent targets (500 Hz;  $p = .12$ ) presented binaurally at 85 dB SPL. Subjects responded with a button press as quickly as possible when, and only when, they heard the infrequent target tone (response hand counterbalanced across blocks).

**ERP Recordings.** As previously detailed<sup>[2]</sup>, ERPs were recorded from 67 scalp sites (ActiView; BioSemi). Continuous EEG data were blink corrected using a spatial, singular value decomposition (NeuroScan). Stimulus-locked epochs (1200 ms, 200 ms prestimulus baseline) were extracted and screened for electrolyte bridges<sup>[7]</sup>. Channels containing artifacts or noise for any given trial were identified using a reference-free approach<sup>[8]</sup>, and replaced by spherical spline interpolations<sup>[9]</sup> when possible. ERP averages were low-pass filtered at 12.5 Hz (-24 dB/octave) and baseline-corrected.

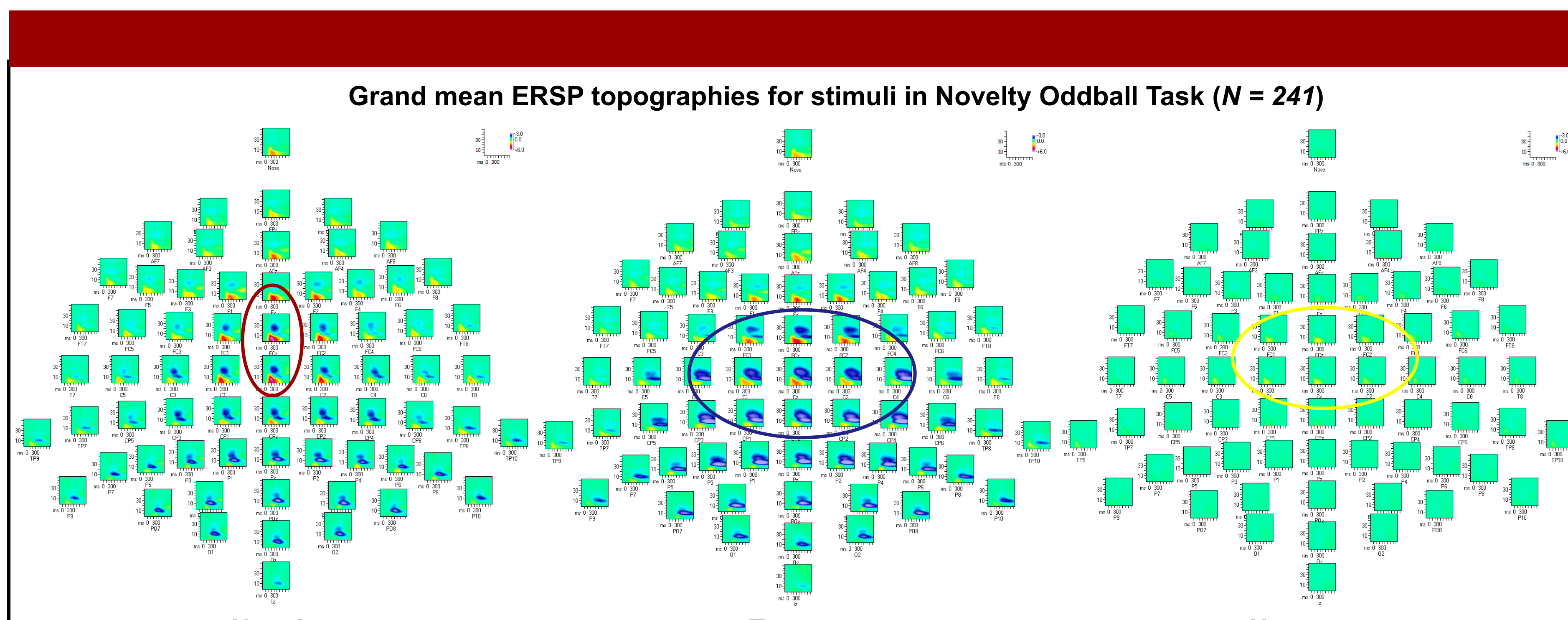
**CSD-tPCA for Novelty Oddball Task.** Reference-free CSD waveforms (spherical spline Laplacian<sup>[9]</sup>) were computed from ERP averages to sharpen topographies, eliminate volume-conducted contributions from distant regions, and quantify underlying current generators<sup>[1,10-12,16]</sup>. CSDs were submitted to unrestricted PCA using the covariance matrix (308 variables = samples -200 to 1000 ms; 48441 observations = [241 subjects x 3 conditions x 67 sites]) followed by Varimax rotation<sup>[13]</sup>.

**CSD-tPCA for Resting EEG.** EEG epochs (2 s; 75% overlap) were transformed to CSD, tapered using a Hanning window, and padded with zeros (1 s at each end) to yield a FFT-transformed spectral resolution of .25 Hz. Amplitude (RMS power) spectra were averaged over all artifact-free epochs for each condition and subject and submitted to tPCA<sup>[3, 12]</sup>.

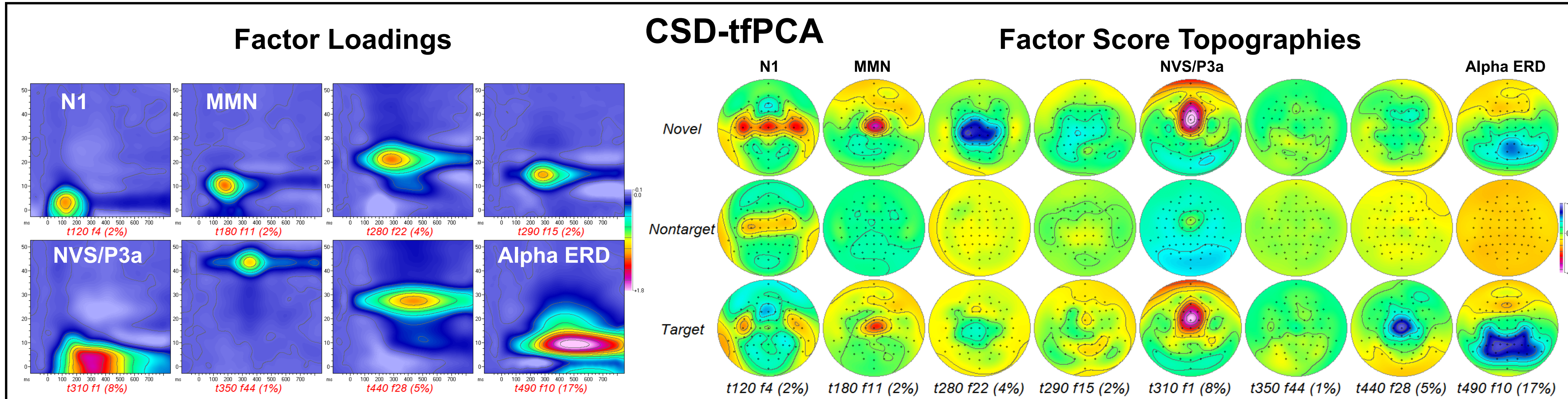
**CSD-tfPCA in Novelty Oddball Task.** ERSPs and corresponding baseline spectra were obtained from CSD-transformed stimulus-locked epochs (-200 to 800 ms) for each electrode, condition (target, nontarget, novel) and participant ( $N = 241$ ) using EegLab<sup>[14]</sup>. For comparability to prior work, ERSP matrices (-70 to 800 ms; 1 to 50 Hz) and baseline spectra were based on FFT-derived log power spectra. Grand mean ERSPs were computed and separately plotted for control and patient groups, and were compared to the time courses of the corresponding averaged CSD and CSD-tPCA loadings waveforms. Analogous to the tPCA and tPCA decompositions, CSD-ERSP matrices were vectorized ( $88 \times 50 = 4400$  variables) and characterized by PCA (i.e., CSD-tfPCA).

**Association of ERSP plots with CSD-tfPCA factors.** Our prior CSD-tfPCA<sup>[2]</sup> identified a component unique to novel stimuli, termed novelty vertex source (NVS; Fig. 1), which was reduced in depressed patients. This a priori knowledge was exploited to delineate the relationship of the ERSP plots with the resulting tPCA factors by comparing CSD-tfPCA solutions stemming from the complete topography or after restricting the ERSP data to midline sites or Cz alone.

**Statistical methods.** For each PCA factor of interest, factor scores were submitted to repeated measures ANOVA using within-subjects factors electrode site and condition (nontarget, target, novel) for midline regions (e.g., vertex), and hemisphere (right/left) for sites off the midline. Treatment (serotonergic, bupropion), treatment response (responder, nonresponder), and gender were between-factors in these ANOVAs. The Beck Depression Inventory (BDI) measure of pretreatment depression was used as a covariate because BDI was correlated with condition-dependent alpha at rest and post-stimulus ERD.



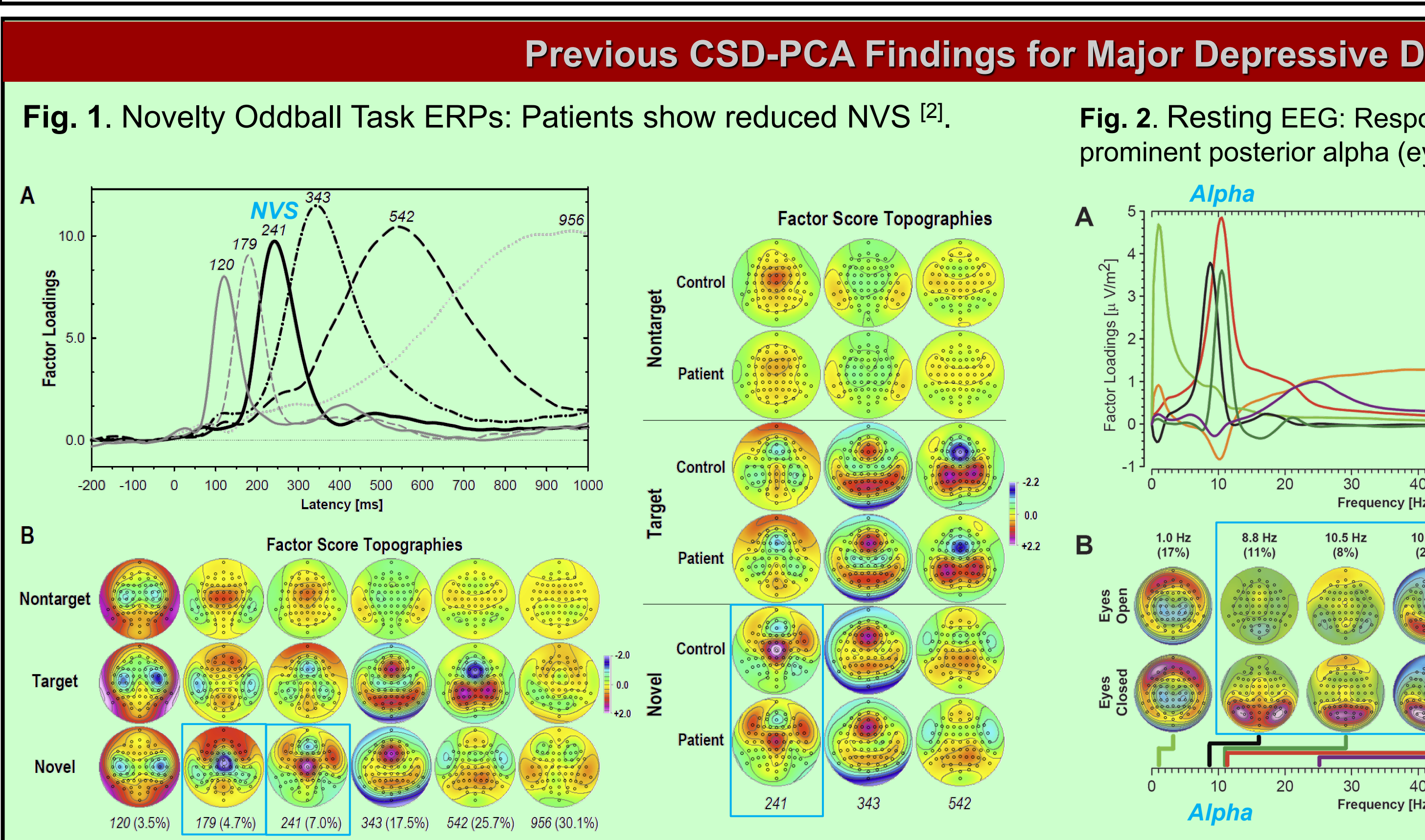
**Fig. 4.** Grand mean ERSP topographies ( $N = 241$ ). For **Novels**, the ERSP follows the time course of the novelty P3, beginning with a prominent low-frequency (alpha and below) ERS that is maximal at central regions at latencies corresponding to the novelty vertex source (NVS<sup>[2]</sup>; red oval). The ERS is followed by a somewhat more broadly distributed beta ERD, and a posterior alpha ERD. For **Targets**, an anterior midline ERS is also observed, although it is less pronounced than for novels, while the subsequent beta ERD is more pronounced and persists to longer latencies. The posterior alpha ERD is also enhanced compared to novels, and is robust at centroparietal sites, stretching to frontocentral sites (i.e., consistent with both posterior alpha and central mu; blue oval). For **Nontargets**, prominent task-related ERSPs were not observed, although evidence of low amplitude ERS corresponding to auditory N1 can be detected (yellow oval).



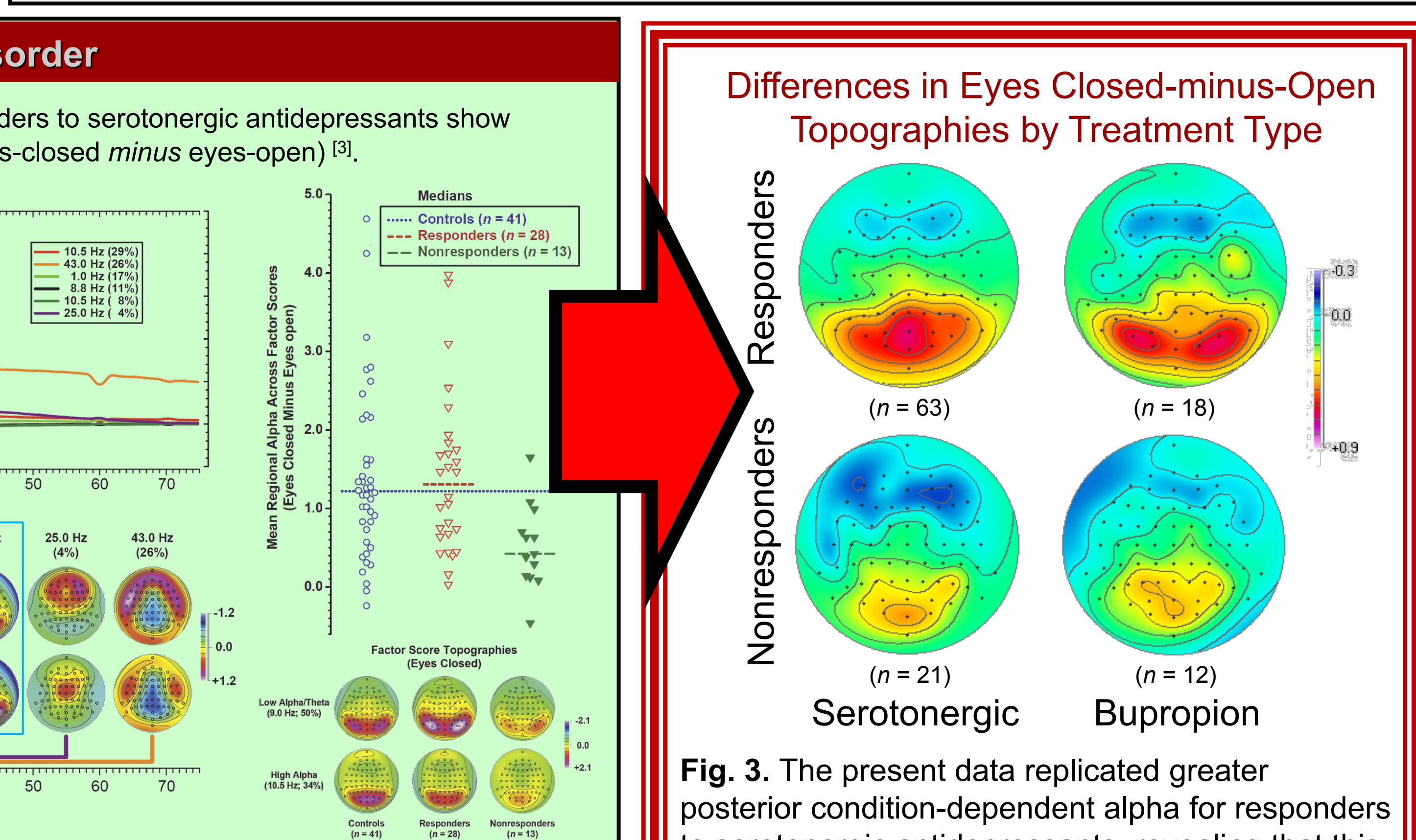
**Fig. 6.** CSD-tfPCA solution ( $N = 241$ ). Factors are sorted by peak latency, showing all high-variance factors with a loadings peak < 500 ms. Factor labels (in red below loadings surfaces) jointly indicate latency ( $t$ ) and frequency ( $f$ ) of the loadings peak (e.g.,  $t120\ f4$  peaks at 120 ms, 4 Hz). The solution identified factors associated with prominent ERS peaks corresponding to the latency of N1, MMN, and NVS/P3a (cf. Figs. 1 and 4). The corresponding factor score topographies illustrate the condition-dependency of these time-frequency components, which compactly describe and quantify the data underlying the ERSP topographies shown in Fig. 4, justifying additional mnemonics (N1, MMN, NVS/P3a, Alpha ERD) to indicate their putative functional properties. The factor identified as Alpha ERD unambiguously quantified alpha desynchronization at 7-12.5 Hz in the latency range of 350-700 ms, showing a posterior topography for novels and targets, but not nontargets (note bilateral extension into central regions for targets).

- ### Conclusions
1. Resting alpha is predictive of a positive outcome to treatment with serotonergic or nonserotonergic (NDRI) antidepressants.
  2. Despite a comparable topography, task-related baseline alpha is selective for bupropion response.
  3. Alpha ERD has a posterior topography for targets and novels, extends to central sensorimotor regions for targets, and is absent for nontargets, but is not related to treatment response.
  4. Frontocentral midline synchronization following infrequent novels and targets at latencies corresponding to MMN and NVS/P3a was greater for serotonergic nonresponders than responders, but patients treated with bupropion showed the opposite difference (i.e., greater ERS in group in which psychomotor slowing has also been found).

**Medial frontocentral and posterior mechanisms are differentially predictive of treatment response to pharmacologic antidepressants**



**Fig. 1.** Novelty Oddball Task ERPs: Patients show reduced NVS<sup>[2]</sup>.

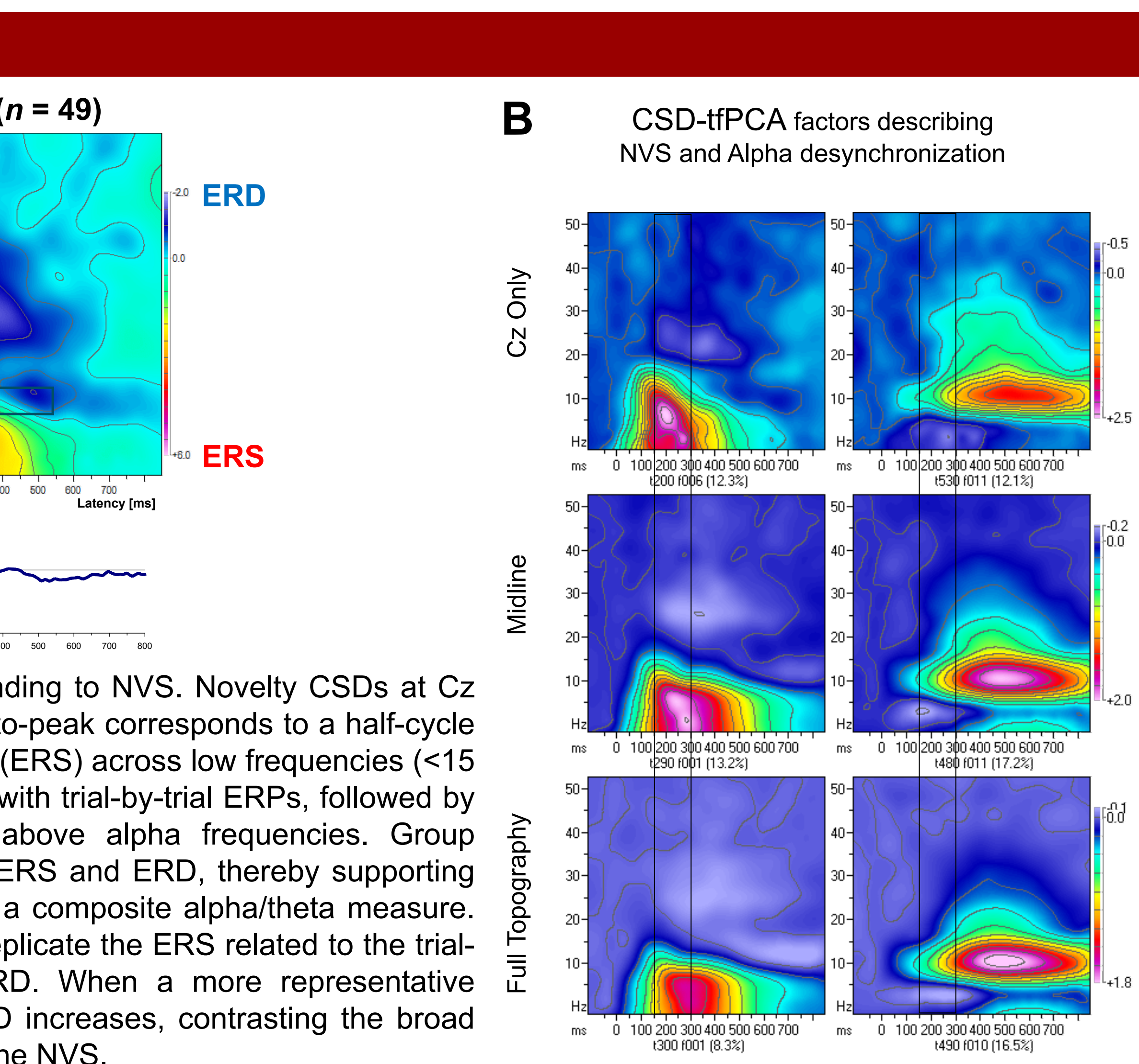


**Fig. 2.** Resting EEG: Responders to serotonergic antidepressants show prominent posterior alpha (eyes-closed minus eyes-open)<sup>[9]</sup>.

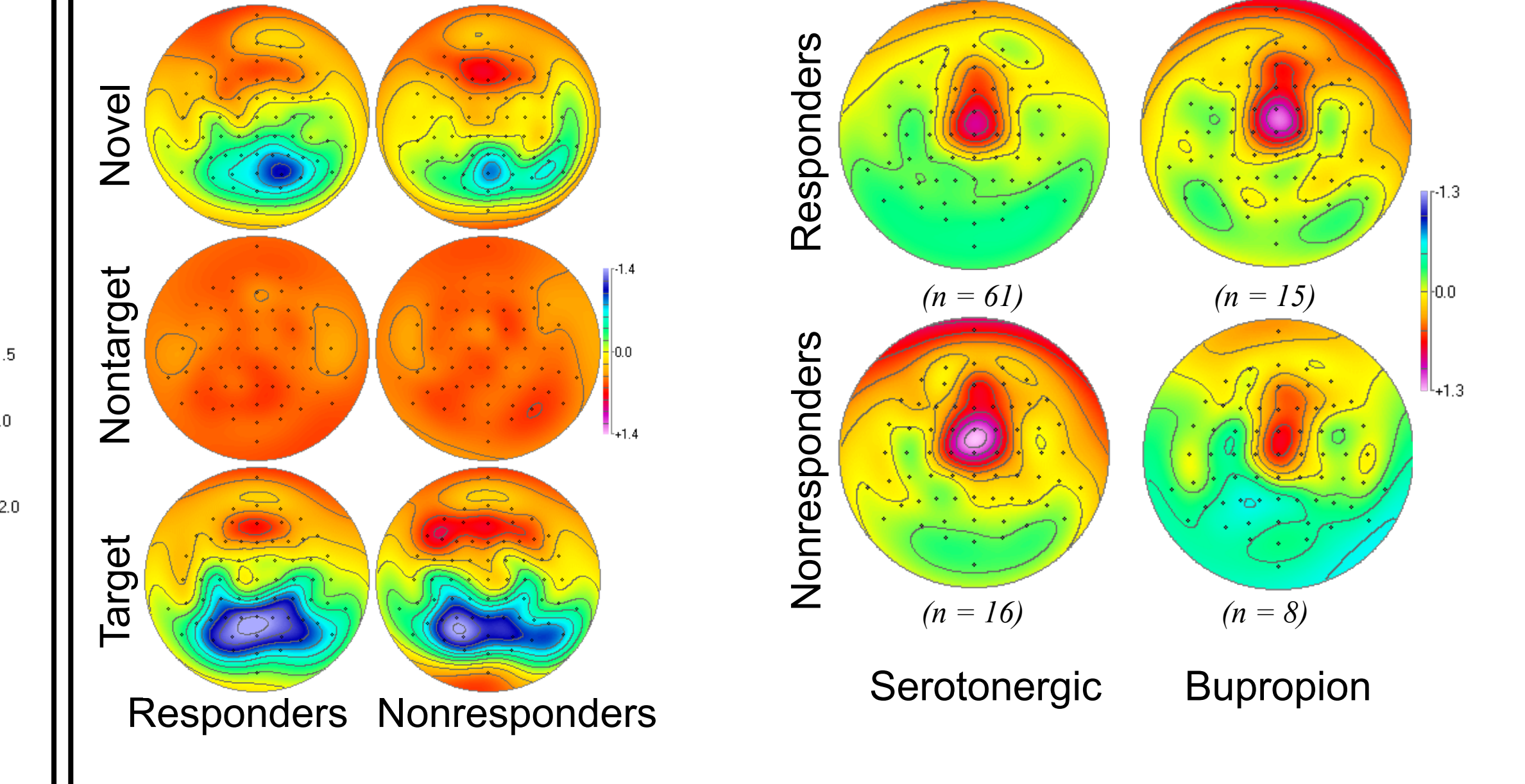
**Table 1. Factor Intercorrelations.**

Factor	Pearson Correlation	MMN ERS		NVS/P3a ERS		Alpha ERD (minus ERS)	
		t120 f4	t180 f11	t1280 f22	t1290 f15	t1310 f1	t1350 f14
Stimulus (tf baseline alpha)	1.000	-.315	-.287	-.202	-.022	.054	.033
rest/2	-.000	.000	.000	.000	.973	.491	.608
rest/12	-.315	1.000	.117	.180	.147	.169	-.045
rest/23	-.000	.000	.011	.005	.015	.023	.024
Age [years]	-.217	.043	.000	-.017	.040	-.200	-.225
BDI	.019	.428	.789	.688	.028	.162	.480
Back Depression Inventory	-.175	.231	.104	.069	.176	-.045	.003
Inventory	.007	.000	.110	.288	.007	.491	.962
Back Depression Inventory (patients only)	-.098	.213	-.005	-.069	.196	-.067	-.052
Inventory	.276	.016	.566	.445	.029	.455	.565
	.125	.123	.125	.125	.125	.125	.125

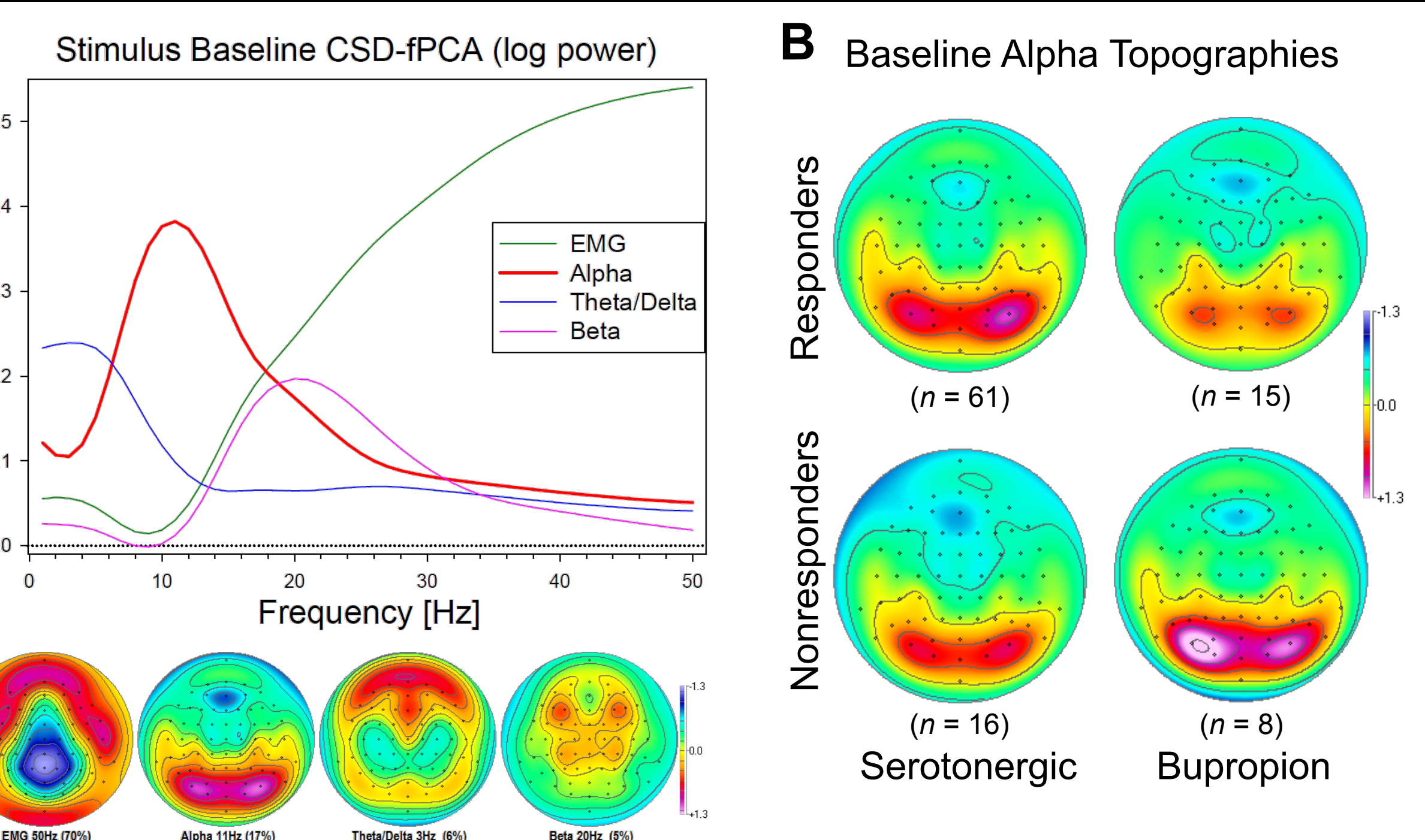
**Fig. 3.** The present data replicated greater posterior condition-dependent alpha for responders to serotonergic antidepressants, revealing that this also applies to bupropion (NDRI) responders.



**Fig. 5.** A. Grand mean ERSPs and CSDs corresponding to NVS. Novelty CSDs at Cz consisted of a sink/source pair at 175/265 ms (peak-to-peak corresponds to a half-cycle sinusoid of 5.6 Hz). An event-related synchronization (ERS) across low frequencies (<15 Hz) closely corresponds to this transition, consistent with trial-by-trial ERPs, followed by an event-related desynchronization (ERD) at and above alpha frequencies. Group differences are evident below 15 Hz, affecting both ERS and ERD, thereby supporting the hypothesized association between the NVS and a composite alpha/theta measure. B. CSD-tfPCA solutions across all conditions at Cz replicate the ERS related to the trial-to-trial ERP, as well as the subsequent alpha ERD. When a more representative topography is provided, the prominence of the ERD increases, contrasting the broad distribution of alpha against the sharp localization of the NVS.



**Fig. 7.** A. Unlike resting EEG, Alpha ERD did not distinguish between responders and nonresponders. B. However, there was a prominent treatment by response interaction ( $p = .015$ ) for ERS following infrequent novels and targets along the frontocentral midline at alpha and theta frequencies at latencies corresponding to mismatch detection (i.e., pooled MMN and NVS/P3a factors).



**Fig. 8.** A. CSD-tfPCA solution for log prestimulus baseline power. Alpha factor score topographies (bottom) are comparable to those from resting EEG (cf. Fig. 3). B. Repeated measures ANOVA revealed a significant treatment by response interaction ( $p < .05$ ) for posterior alpha: Bupropion responders ( $n = 15$ ) showed markedly less alpha than nonresponders ( $n = 8$ ), while serotonergic responders and nonresponders did not differ.

### References

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BDI: Inversely related to tf baseline alpha (only when controls included)  
 \*MMN: broad pattern of intercorrelation (all conditions)  
 +: Inversely related to ERS at MMN latencies for nontargets  
 -: Positively related to ERS at MMN latencies for nontargets  
 #3a: only correlated with NVS/P3a factors (all conditions)  
 #NVS: only correlated with NVS/P3a factors (all conditions)